

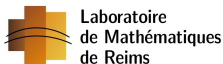
A contrast source inversion method for the reconstruction of electrical properties

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Journée Ondes des poètes, Avril 17–19, ENSTA

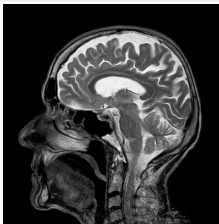


Funding from ANR ELECTRA, grant ANR-21-CE19-0040.

- Medical context
- The forward problem
- Contrast source inversion
- Conclusion

Aim

Reconstruct the **electrical properties (permittivity and conductivity)** of the tissues in the human brain from **radio-frequency measurements** obtained by **magnetic resonance imaging (MRI)**.



- ↪ disease detection
- ↪ safety standards

ANR Project ELECTRA : IADI (INSERM, Nancy), CHRU Nancy, Healtis (Nancy), ICUBE (Strasbourg), LMR (Reims)

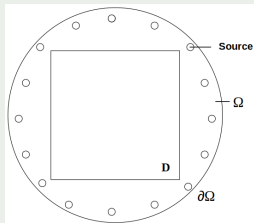
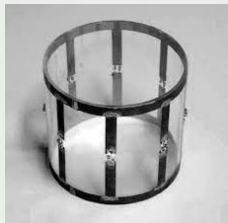
numerical methods for precise reconstruction of electric properties & database with respect to age

Magnetic resonance imaging (MRI)

Principle :

- strong static magnetic field \mathbf{B}_0 , e.g. 3T
 - excitation of hydrogen protons through radiofrequency (RF) pulse at **Larmor frequency**, e.g. 128 MHz at 3T
 - emission of e.m. signal when protons return to initial state
- ⇒ picture of biological tissues containing water

Birdcage coil : a typical configuration of RF antenna



$\Omega \rightsquigarrow$ computational domain

$D \subset \Omega \rightsquigarrow$ measurement area

line source field from 8 or 16 legs (outside D)

time-harmonic Maxwell's equations at fixed angular frequency ω with linear isotropic constitution laws, Ohm's law and **scaling** wrt electric permittivity ε_0 and magnetic permeability μ_0 in free space

$$\Rightarrow \quad \mathcal{E}(\mathbf{x}, t) = \Re e \left(e^{-i\omega t} \sqrt{\varepsilon_0} \mathbf{E} \right), \quad \mathcal{H}(\mathbf{x}, t) = \Re e \left(e^{-i\omega t} \sqrt{\mu_0} \mathbf{H} \right)$$

$$\begin{aligned} -ik\varepsilon_r \mathbf{E} - \text{curl } \mathbf{H} &= -\sqrt{\mu_0} \mathbf{J}_s \\ -ik\mu_r \mathbf{H} + \text{curl } \mathbf{E} &= 0 \end{aligned}$$

with source term \mathbf{J}_s , wave number $k = \omega \sqrt{\varepsilon_0 \mu_0}$ and relative electromagnetic parameters

$$\varepsilon_r = \frac{1}{\varepsilon_0} \left(\varepsilon + \frac{i\sigma}{\omega} \right), \quad \mu_r = \frac{\mu}{\mu_0}.$$

Elimination of \mathbf{H} :

$$\operatorname{curl} \mu_r^{-1} \operatorname{curl} \mathbf{E} - k^2 \varepsilon_r \mathbf{E} = ik \sqrt{\mu_0} \mathbf{J}_s$$

Two-dimensional transverse magnetic setting and $\mu_r = 1$:

$$\mathbf{E} = \begin{pmatrix} 0 \\ 0 \\ E \end{pmatrix}, \mathbf{J}_s = \begin{pmatrix} 0 \\ 0 \\ j_s \end{pmatrix} \Rightarrow -\Delta E - k^2 \varepsilon_r E = \underbrace{ik \sqrt{\mu_0} j_s}_{\stackrel{\text{def}}{=} F}$$

Perfect conductor boundary condition in a bounded domain Ω :

$$\begin{cases} -\Delta E - k^2 \varepsilon_r E = F & \text{in } \Omega, \\ E = 0 & \text{on } \partial\Omega. \end{cases}$$

Perturbation due to the presence of an object

Assume that $k^2 \notin \text{sp}(-\Delta^{\text{Dir}})$.

Reference configuration : no object $\Rightarrow \varepsilon_r = 1$. Source term F .

$$\begin{cases} -\Delta E^{\text{ref}} - k^2 E^{\text{ref}} &= F & \text{in } \Omega, \\ E^{\text{ref}} &= 0 & \text{on } \partial\Omega. \end{cases} \quad (1)$$

Configuration with object : assume that $\text{supp}(1 - \varepsilon_r) \subset D$ where $D \subset \Omega$. $\exists m \varepsilon_r > 0$ on some part of D . **Same** source term F .

$$\begin{cases} -\Delta E^{\text{tot}} - k^2 \varepsilon_r E^{\text{tot}} &= F & \text{in } \Omega, \\ E^{\text{tot}} &= 0 & \text{on } \partial\Omega. \end{cases} \quad (2)$$

Forward problem

Let E^{ref} be the solution to (1) for given F .

For **given** ε_r , find the **scattered field** $E^{\text{sc}} = E^{\text{tot}} - E^{\text{ref}}$, solution to

$$\begin{cases} -\Delta E^{\text{sc}} - k^2 \varepsilon_r E^{\text{sc}} &= -k^2(1 - \varepsilon_r) E^{\text{ref}} & \text{in } \Omega, \\ E^{\text{sc}} &= 0 & \text{on } \partial\Omega. \end{cases} \quad (3)$$

Which formulation for the inverse problem ?

Inverse problem as a parameter problem

Let E^{ref} be the solution to (1) for given F .

For **given measurements** f^{data} on $D \subset \Omega$, find ε_r such that the scattered field E^{sc} , solution to (3), satisfies $E^{\text{sc}}|_D = f^{\text{data}}$.

\rightsquigarrow resolution by minimization of a least square functional of the data error.

Difficulty : inverse parameter problem, the differential operator in (3) depends on ε_r .

$$\begin{cases} -\Delta E^{\text{sc}} - k^2 \varepsilon_r E^{\text{sc}} = -k^2(1 - \varepsilon_r) E^{\text{ref}} & \text{in } \Omega, \\ E^{\text{sc}} = 0 & \text{on } \partial\Omega. \end{cases}$$

Reformulation of problem (3)

$$\begin{cases} -\Delta E^{\text{sc}} - k^2 E^{\text{sc}} = -k^2(1 - \varepsilon_r) E^{\text{tot}} & \text{in } \Omega, \\ E^{\text{sc}} = 0 & \text{on } \partial\Omega. \end{cases} \quad (4)$$

Inverse problem as a non-linear source problem

Let E^{ref} be the solution to (1) for given F .

For **given measurements** f^{data} on $D \subset \Omega$, find $(\varepsilon_r, E^{\text{tot}})$ defined on Ω , such that the scattered field E^{sc} , solution to (4), satisfies the following system

$$\begin{cases} E^{\text{sc}}|_D = f^{\text{data}} & \text{[data equation]} \\ E^{\text{ref}} + E^{\text{sc}} = E^{\text{tot}} & \text{[state equation]} \end{cases}$$

\rightsquigarrow resolution by minimization of a least square functional of the weighted data and state error.

The inverse problem as contrast source inversion

Let $\chi = 1 - \varepsilon_r$ the **contrast function** and $w = \chi E^{\text{tot}}$ the **contrast source**.

$$\text{Problem (4)} \Rightarrow -\Delta E^{\text{sc}} - k^2 E^{\text{sc}} = -k^2 \underbrace{(1 - \varepsilon_r) E^{\text{tot}}}_{= \chi E^{\text{tot}} \stackrel{\text{def}}{=} w} \text{ in } \Omega.$$

Linear solution operator

$$\begin{aligned} \mathcal{L}_b : L^2(\Omega) &\rightarrow H_0^1(\Omega) \\ w &\mapsto E^{\text{sc}} \end{aligned}$$

where $E^{\text{sc}} \in H_0^1(\Omega)$ is the (variational) solution to

$$\begin{cases} -\Delta E^{\text{sc}} - k^2 E^{\text{sc}} = -k^2 w & \text{in } \Omega, \\ E^{\text{sc}} = 0 & \text{on } \partial\Omega. \end{cases} \quad (5)$$

The inverse problem as contrast source inversion

Let $\mathcal{R}_D : L^2(\Omega) \rightarrow L^2(D)$ be the **restriction operator** to $D \subset \Omega$.

Recall that $\chi = 1 - \varepsilon_r$ and $w = \chi E^{\text{tot}}$.

Operator formulation of the data and state equation :

$$\begin{aligned} E|_D^{\text{sc}} = f^{\text{data}} &\Rightarrow \mathcal{R}_D \circ \mathcal{L}_b(w) = f^{\text{data}} \\ E^{\text{ref}} + E^{\text{sc}} = E^{\text{tot}} &\Rightarrow \chi (E^{\text{ref}} + \mathcal{L}_b(w)) = w \end{aligned}$$

Inverse problem as contrast source inversion (CSI)

Let E^{ref} be the solution to (1) for given F .

For **given measurements** f^{data} on $D \subset \Omega$, find (χ, w) defined on Ω , such that

$$\begin{cases} \mathcal{R}_D \circ \mathcal{L}_b(w) = f^{\text{data}} & \text{[data equation]} \\ \chi (E^{\text{ref}} + \mathcal{L}_b(w)) = w & \text{[state equation]} \end{cases}$$

Seminal paper of van den Berg/Kleinman, Inv. Pb., 1997

- reconstruction of the complex refraction index of an object from surface measurements outside the object
- ⇒ scalar scattering problem in an unbounded domain
- solution operator based on Green's function

Unbounded domain, MRI-EPT

- Balidemaj et al., IEEE Trans. Medical Imaging, 2016
- Arduino et al., Inv. Pb., 2018

Bounded domain - FEM

- Zakaria et al., Inv. Pb., 2010 (microwave imaging, Helmholtz equation)
- Arduino et al., IEEE Trans. Medical Imaging, 2021 (MRI-EPT)

Cost function

$$\mathcal{F}(\chi, w) = \mathcal{F}^{\text{data}}(w) + \mathcal{F}^{\text{state}}(\chi, w) \longrightarrow \min$$

$$\text{with } \mathcal{F}^{\text{data}}(w) = \frac{\eta^{\text{data}}}{2} \|f^{\text{data}} - (\mathcal{R}_D \circ \mathcal{L}_b)(w)\|_{0,D}^2,$$

$$\mathcal{F}^{\text{state}}(\chi, w) = \frac{\eta^{\text{state}}}{2} \|\chi(E^{\text{ref}} + \mathcal{L}_b(w)) - w\|_{0,D}^2,$$

for any $\chi \in L^\infty(\Omega)$ and $w \in L^2(\Omega)$ and normalization constants $\eta^{\text{data}} > 0$ and $\eta^{\text{state}} > 0$.

Two-step iterative method :

- update w_n by a gradient-based method $\rightsquigarrow w_{n+1}$
- update χ_n from knowledge of w_{n+1}

Adjoint solution operator

$$\begin{aligned} \mathcal{L}_b^* : H^{-1}(\Omega) &\rightarrow L^2(\Omega) \\ \varphi &\mapsto -k^2 p, \end{aligned}$$

where the **adjoint state** $p \in H_0^1(\Omega)$ is the variational solution of

$$\begin{cases} -\Delta p - k^2 p = \varphi & \text{in } \Omega, \\ p = 0 & \text{on } \partial\Omega. \end{cases} \quad (6)$$

Then $(\mathcal{R}_D \circ \mathcal{L}_b)^*$ is defined with the help of the extension operator $\mathcal{R}_D^* : L^2(D) \rightarrow L^2(\Omega)$ given by

$$\mathcal{R}_D^*(\varphi) = \begin{cases} \varphi & \text{on } D \\ 0 & \text{on } \Omega \setminus \bar{D}. \end{cases}$$

Computation of the gradient by the adjoint state

$$\mathcal{F}^{\text{data}}(w) = \frac{\eta^{\text{data}}}{2} \|f^{\text{data}} - (\mathcal{R}_D \circ \mathcal{L}_b)(w)\|_{0,D}^2,$$

$$\mathcal{F}^{\text{state}}(\chi, w) = \frac{\eta^{\text{state}}}{2} \|\chi(E^{\text{ref}} + \mathcal{L}_b(w)) - w\|_{0,D}^2,$$

Formula for the gradient wrt w

$$\nabla_w \mathcal{F}^{\text{data}}(w) = -\eta^{\text{data}} \Re \{ (\mathcal{R}_D \circ \mathcal{L}_b)^*(\rho) \}$$

$$\nabla_w \mathcal{F}^{\text{state}}(\chi, w) = -\eta^{\text{state}} \Re \{ r - \mathcal{L}_b^*(\bar{\chi} r) \}$$

where $\rho = f^{\text{data}} - (\mathcal{R}_D \circ \mathcal{L}_b)(w)$ is the data error and $r = \chi(E^{\text{ref}} + \mathcal{L}_b(w)) - w$ is the state error which is taken into account only on the subdomain D .

Computation of the contrast function from given w

For a given contrast source w , the total field E^{tot} can be computed by

$$E^{\text{tot}} = E^{\text{ref}} + \mathcal{L}_b(w).$$

Then the contrast function

$$\chi = \frac{w}{E^{\text{tot}}} = \frac{w \overline{E^{\text{tot}}}}{|E^{\text{tot}}|^2} \quad (7)$$

satisfies the state equation

$$\chi (E^{\text{ref}} + \mathcal{L}_b(w)) = w.$$

NB : For χ defined from w and E^{tot} by (7), the state error $r = \chi(E^{\text{ref}} + \mathcal{L}_b(w)) - w$ vanishes. Thus,

$$\nabla_w \mathcal{F}^{\text{state}}(\chi, w) = -\eta^{\text{state}} \Re \{ r - \mathcal{L}_b^*(\bar{\chi} r) \} = 0.$$

Data : E^{ref} , k , f^{data} . **Initial data :** w_0 , χ_0

Initialization : compute $E_0^{\text{sc}} = \mathcal{L}_b(w_0)$ and initial direction $v_0 = -g_0$

1 Update :

- compute $\mathcal{L}_b(v_n)$
- compute optimal step α_n (explicit formula depending on $\mathcal{L}_b(v_n)$)
- update contrast source : $w_{n+1} = w_n + \alpha_n v_n$
- solve direct problem : $E_{n+1}^{\text{sc}} = E_n^{\text{sc}} + \alpha_n \mathcal{L}_b(v_n)$
- compute total field : $E_{n+1}^{\text{tot}} = E^{\text{ref}} + E_{n+1}^{\text{sc}}$
- compute new contrast function χ_{n+1} from formula (7)

2 Compute new residual and gradient :

- $\rho_{n+1} = f^{\text{data}} - E_{n+1}^{\text{sc}}|_D$
- $g_{n+1} = -\eta^{\text{data}} \Re \{ (\mathcal{R}_D \circ \mathcal{L}_b)^* [\rho_{n+1}] \}$

3 Non-linear conjugate gradient (Polak-Ribière) direction :

- $v_{n+1} = -g_{n+1} + \frac{\langle g_{n+1}, g_{n+1} - g_n \rangle_D}{\langle g_n, g_n \rangle_D} v_n$

First numerical results for synthetic electric field data

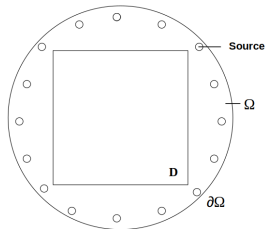


Figure – Configuration of a birdcage coil

Line source field

$$j_s(\mathbf{x}) = \sqrt{I} \sum_{\ell=1}^{16} \frac{e^{ikr_\ell}}{\sqrt{r_\ell}}$$

with intensity I and $r_\ell = \|\mathbf{x} - \mathbf{c}_\ell\|$ the distance to the center \mathbf{c}_ℓ of the ℓ th leg.

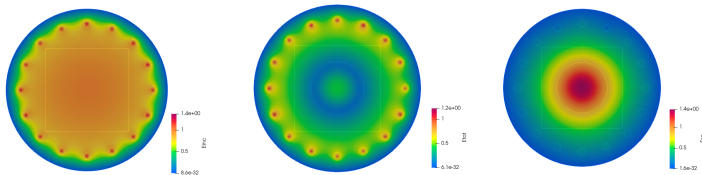


Figure – E^{ref} (without object, right), E^{tot} (with object, middle), E^{sc} (scattered field, right), P1 FEM - FreeFem++

First numerical results for synthetic electric field data

Reconstruction of a homogeneous circular object with relative permittivity $\varepsilon_r = 52.5 + 48.028i$ (white matter at 128 [MHz]).

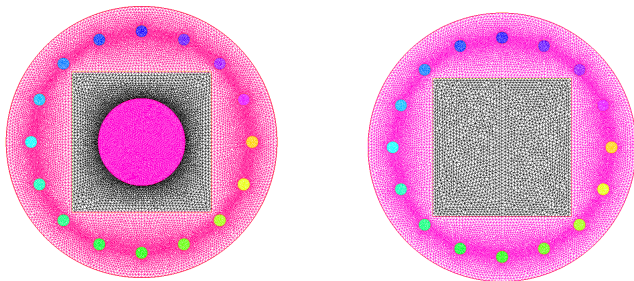


Figure – Mesh for data generation (left). Mesh for CSI algorithm (right), ≈ 2000 measurement points.

Reconstructed mean value of ε_r in the object : $51.98 + 47.26i$
 $\rightsquigarrow \approx 1\%$ relative error for noiseless data

Noisy data

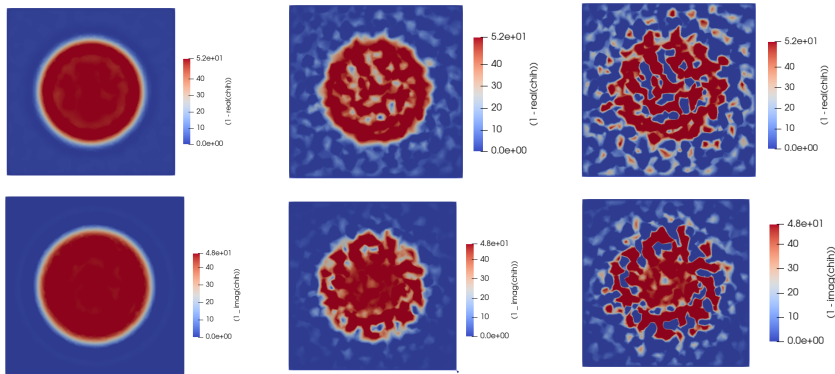


Figure – Noiseless data (left column). Noisy data with 0.5% (middle), 2% (right column). Upper line : real part of ϵ_r . Lower line : imaginary part of ϵ_r .

Realistic 2D head model

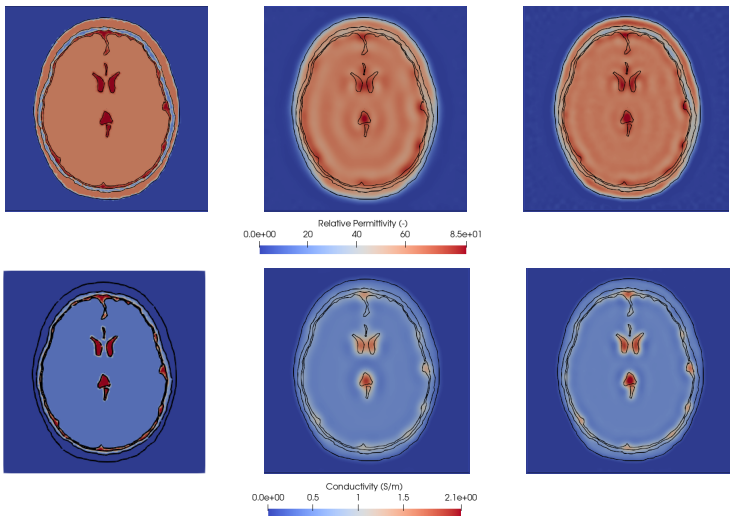


Figure – Permittivity (upper line) and conductivity (lower line). Noiseless data. Ground truth (left). 5000 iter. (middle). 20 000 iter. (right).

What does MRI really measure ?

MRI does not measure the electric field, but the B_1^+ -field related to the **scattered magnetic field**.

Maxwell's equations ($\mu_r = 1$) \rightsquigarrow $\text{curl } \mathbf{E} = ik\mathbf{H}$

$$\text{in 2D : } \mathbf{H} = -\frac{i}{k} \text{curl } E = -\frac{i}{k} \begin{pmatrix} \partial_y E \\ -\partial_x E \end{pmatrix}.$$

MRI measurements

$$B_1^+ \stackrel{\text{def}}{=} \frac{H_x^{\text{sc}} + iH_y^{\text{sc}}}{2} \text{ on } D$$

Operator formulation of the data error with B_1^+ -data

Define linear operators \mathcal{C} and \mathcal{P} by

Curl operator \mathcal{C}

$$\begin{aligned} \mathcal{C} : H_0^1(\Omega) &\rightarrow L^2(\Omega)^2 \\ E^{\text{sc}} &\mapsto -\frac{i}{k} \mathbf{curl} E^{\text{sc}}. \end{aligned}$$

B_1^+ -operator \mathcal{P}

$$\begin{aligned} \mathcal{P} : L^2(\Omega)^2 &\rightarrow L^2(\Omega) \\ \mathbf{u} &\mapsto \frac{u_x + iu_y}{2}. \end{aligned}$$

Then, the **data operator** \mathcal{S}^+ is defined from composition by

$$\begin{aligned} \mathcal{S}^+ : L^2(\Omega) &\rightarrow L^2(D) \\ w &\mapsto (\mathcal{R}_D \circ \mathcal{P} \circ \mathcal{C} \circ \mathcal{L}_b)(w) \end{aligned}$$

Adjoint B_1^+ -operator \mathcal{P}^*

$$\begin{aligned} \mathcal{P}^* : L^2(\Omega) &\rightarrow L^2(\Omega)^2 \\ \varphi &\mapsto \frac{1}{2} \begin{pmatrix} \varphi \\ -i\varphi \end{pmatrix}. \end{aligned}$$

Adjoint curl operator \mathcal{C}^*

$$\begin{aligned} \mathcal{C}^* : L^2(\Omega)^2 &\rightarrow H^{-1}(\Omega) \\ \mathbf{v} &\mapsto +\frac{i}{k} \mathbf{curl} \mathbf{v}. \end{aligned}$$

with $\mathbf{curl} \mathbf{v} = \partial_x v_y - \partial_y v_x$.

The adjoint data operator

Data operator

$$\begin{aligned} \mathcal{S}^+ : L^2(\Omega) &\rightarrow L^2(D) \\ w &\mapsto (\mathcal{R}_D \circ \mathcal{P} \circ \mathcal{C} \circ \mathcal{L}_b)(w) \end{aligned}$$

$$\mathcal{S}^{+,*} = (\mathcal{L}_b^* \circ \mathcal{C}^* \circ \mathcal{P}^* \circ \mathcal{R}_D^*) : L^2(D) \rightarrow L^2(\Omega)$$

Let $\varphi \in L^2(D)$. Then, $\mathcal{S}^{+,*}(\varphi) = -k^2 p$ where p is the (variational) solution of

$$\begin{cases} -\Delta p - k^2 p = \frac{i}{k} \operatorname{curl} \mathbf{v} & \text{in } \Omega, \\ p = 0 & \text{on } \partial\Omega. \end{cases} \quad (8)$$

where

$$\mathbf{v} = \mathcal{P}^*(\mathcal{R}_D^*(\varphi)) = \begin{cases} \frac{1}{2} \begin{pmatrix} \varphi \\ -i\varphi \end{pmatrix} & \text{on } D, \\ \mathbf{0} & \text{on } \Omega \setminus \overline{D}. \end{cases}$$

Cost function for B_1^+ -data

$$\mathcal{F}(\chi, w) = \mathcal{F}^{\text{data},+}(w) + \mathcal{F}^{\text{state}}(\chi, w) \longrightarrow \min$$

$$\text{with } \mathcal{F}^{\text{data},+}(w) = \frac{\eta^{\text{data}}}{2} \|B_1^{+, \text{data}} - \mathcal{S}^+(w)\|_{0,D}^2,$$

$$\mathcal{F}^{\text{state}}(\chi, w) = \frac{\eta^{\text{state}}}{2} \|\chi(E^{\text{ref}} + \mathcal{L}_b(w)) - w\|_{0,D}^2,$$

Formula for the gradient wrt w

$$\nabla_w \mathcal{F}^{\text{data},+}(w) = -\eta^{\text{data}} \Re \{ \mathcal{S}^{+,*}(\rho^+) \}$$

$$\nabla_w \mathcal{F}^{\text{state}}(\chi, w) = -\eta^{\text{state}} \Re \{ r - \mathcal{L}_b^*(\bar{\chi}r) \}$$

where $\rho^+ = B_1^{+, \text{data}} - \mathcal{S}^+(w)$ is the data error for B_1^+ -data and $r = \chi(E^{\text{ref}} + \mathcal{L}_b(w)) - w$ is the state error (unchanged).

Finite Element Solver

FreeFem



F. Hecht, J. Num. Math., 2012.

Choice of Finite Elements ?

- Solution operator \mathcal{L}_b and its adjoint \mathcal{L}_b^* :
- ↪ discretize E^{sc} and p by **Lagrange Finite Elements of type P1**
- Restriction/extension operators \mathcal{R}_D and \mathcal{R}_D^* :
- ↪ implement the subdomain $D \subset \Omega$ as a **region**
- Implementation of the adjoint curl operator \mathcal{C}^* :



A. Arduino et al., IEEE Trans. Medical Imaging, 2017.

use Stokes' Theorem on a dual mesh and discretize $\mathcal{C}^* \mathbf{v}$ by Lagrange Finite Elements of type P1 with nodal values

$$(\mathcal{C}^* \mathbf{v})_I \stackrel{\text{def}}{=} \int_{G_I} \mathcal{C}^* \mathbf{v} \, dx = \frac{i}{k} \oint_{\partial G_I} \mathbf{v} \cdot \boldsymbol{\tau} \, ds$$

Implementation of the adjoint curl operator

\mathcal{C}^* is involved in the r.h.s. of the adjoint problem :

$$\begin{cases} -\Delta p - k^2 p &= \frac{i}{k} \operatorname{curl} \mathbf{v} & \text{in } \Omega, \\ p &= 0 & \text{on } \partial\Omega. \end{cases}$$

Variational formulation : Find $p \in H_0^1(\Omega)$ s.t.

$$a(q, p) = \langle q, \frac{i}{k} \operatorname{curl} \mathbf{v} \rangle_{H_0^1(\Omega), H^{-1}(\Omega)} \quad \forall q \in H_0^1(\Omega),$$

where

$$a(q, p) = \int_{\Omega} \nabla q \cdot \nabla \bar{p} \, dx - k^2 \int_{\Omega} q \bar{p} \, dx \quad \forall p, q \in H_0^1(\Omega).$$

$$\langle q, \frac{i}{k} \operatorname{curl} \mathbf{v} \rangle_{H_0^1(\Omega), H^{-1}(\Omega)} = -\frac{i}{k} \int_{\Omega} \operatorname{curl} q \cdot \bar{\mathbf{v}} \, dx$$

\rightsquigarrow discretize p and q by **Lagrange Finite Elements of type P1**

Numerical results for B_1^+ -data

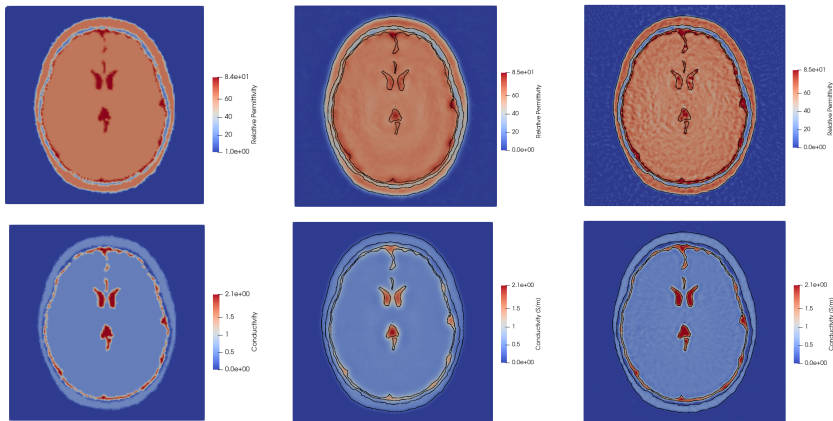
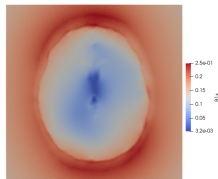


Table – Permittivity (upper line). Conductivity (lower line). Ground truth (left). Reconstruction after 40 (middle) and 100 (right) iterations. Refined mesh, $\approx 27\,000$ measurement points.

- Reconstruction of EPs ε and σ in various academic and realistic configurations.
- Good performance for noiseless data and electric measurements.
- First step towards realistic B_1^+ -data.



$|B_1^+|$

In (near) future

- (Multiplicative) regularization of CSI [cf. Balidemaj et al 2016]
- Phaseless data : $|B_1^+|$ instead of full B_1^+ data [cf. Arduino et al. 2018]
- Experimental data of a phantom [IADI, Nancy]

